

Intrinsically magnetic susceptibility in human blood and its impact on cell separation: Non-classical and intermediate monocytes have the strongest magnetic behavior in fresh human blood

Jenifer Gómez-Pastora[§], James Kim[§], Victor Multanen[§], Mitchell Weigand[§], Nicole A. Walters[§], Eduardo Reátegui[§], Andre F. Palmer[§], Mark H. Yazer[#], Maciej Zborowski[€], Jeffrey J. Chalmers^{§,*}

[§]William G. Lowrie Department of Chemical and Biomolecular Engineering, The Ohio State University, 151 West Woodruff Avenue, Columbus, OH 43210

[#]Department of Pathology, University of Pittsburgh, 3636 Blvd of the Allies, Pittsburgh, PA 15213

[€]Department of Biomedical Engineering, Cleveland Clinic, 9500 Euclid Avenue, Cleveland, OH 44195

Grant number: 1R01HL131720-01A1

*Corresponding Author:

Jeffrey J. Chalmers

William G. Lowrie Department of Chemical and Biomolecular Engineering

The Ohio State University

151 West Woodruff Avenue, Columbus, OH 43210

Phone: (614) 292-2727

Email: chalmers.1@osu.edu

ABSTRACT

The presence of iron in circulating monocytes is well known as they play an essential role in iron recycling. It has been demonstrated that the iron content of blood cells can be measured through their magnetic behavior; however, the magnetic properties of different monocyte subtypes remain unknown. In this study, we report for the first time, the magnetic behavior of classical, intermediate and non-classical monocytes, which is related to their iron storage capacity. The magnetic properties of monocytes were compared to other blood cells, such as lymphocytes and red blood cells in the oxyhemoglobin and methemoglobin states, and a cancer cell type. For this analysis, we used an instrument referred to as Cell Tracking Velocimetry (CTV), which quantitatively characterizes the magnetic behavior of biological entities. Our results demonstrate that significant fractions of the intermediate and non-classical monocytes have high magnetophoretic mobilities, equivalent to methemoglobin red blood cells and higher than the classical subset, suggesting their higher iron storage capacities. Moreover, our findings have implications for the immunomagnetic separation industry; we demonstrate that negative magnetic isolation techniques for recovering monocytes from blood should be used with caution, as it is possible to lose magnetic monocytes when using this technique.

Keywords: monocytes, magnetic susceptibility, cell tracking velocimetry, immunomagnetic separation

INTRODUCTION

Monocytes are circulating blood cells that account for fewer than 10% of the total number of leukocytes (Sprangers et al., 2016). Despite their low concentration in blood, they play important roles in the immune system (Kratofil et al., 2017), and their isolation with high purity is necessary for many research applications. Some of the techniques used to separate them from other cells in the blood are magnetic-based and rely on the assumption that these cells are “non-magnetic” (Bhattacharjee et al., 2017), even though the presence of iron in monocytes is well known as they are involved in iron recycling (Weiss, 2009). In our previous report (Kim et al., 2019), we characterized for the first time the magnetic behavior of CD14⁺ monocytes, presenting a new way to quantify iron storage through magnetic mobility, which has the potential to provide new insight into iron recycling pathways in clinical samples. By measuring the magnetic properties of human monocytes, platelets and red blood cells (RBCs) in the oxyhemoglobin (oxyHb-RBCs) and methemoglobin (metHb-RBCs) states, we demonstrated that a monocyte fraction reported the highest magnetic mobility.

In humans, three circulating monocyte subsets are classified based on expression levels of CD14 and CD16: classical (CD14⁺⁺ CD16⁻), intermediate (CD14⁺⁺ CD16⁺) and non-classical (CD14⁺ CD16⁺⁺), with relative proportions of 85%, 5% and 10%, respectively. These subsets have distinct features: different half-lives in circulation, phagocytic activity and production of inflammatory cytokines (Kawamura & Ohteki, 2018). As a result of these different phenotypes, their role in iron storage and recycling is presumably different. Nevertheless, the magnetic properties of the different monocyte subtypes remain unknown.

It has been suggested that it is possible that monocytes can be contaminated with attached platelets during CD14 sorting in a flow cytometer. In our previous work (Kim et al., 2019), we demonstrated that we could, in fact, by fluorescence-activated cell sorting (FACS), separate the monocytes into subfractions with and without attached platelets. Nevertheless, we independently separated platelets and

demonstrated that platelets are not magnetic and no difference in magnetic susceptibility was observed in these two subtypes. Surprisingly, however, we noticed other significantly entities (smaller than typical blood cells) in the purely monocyte fraction that were negative for platelet markers (as indicated by flow and image cytometry). Finally, it has also been suggested that at least one type of monocyte subtypes, non-classical, can be contaminated with NK and B cells during sorting (Marimuthu et al., 2018).

In this work, we report the magnetic behavior of the three monocyte subsets, which are related to their ability to store iron, and further characterize these subtypes. Further, we compare the magnetic susceptibility of these monocyte subtypes to the magnetic susceptibility of other blood cells as well as a number of cancer cell types. We also discuss the implications of these magnetic susceptibilities to their separation using common magnetic cell separation systems, such as magnetic columns packed with spherical steel balls (i.e. MACS® Columns from Miltenyi Biotec).

EXPERIMENTAL SECTION

For the monocyte subset study, blood from five healthy subjects (two females and three males) was collected with informed consents according to a protocol approved by the Institutional Review Board from The Ohio State University (protocol 2018H0268). Peripheral blood mononuclear cells (PBMCs) and RBCs were collected from 40 mL of whole blood by performing a Ficoll density gradient centrifugation. RBCs were washed with phosphate buffered saline (PBS) and converted into methHb-RBCs via incubation with sodium nitrite (NaNO_2), as presented in **Figure 1**.

The 3 monocyte subsets were isolated from PBMCs by fluorescence-activated cell sorting using a BD FACS ARIA. Briefly, PBMCs (containing around 20 million monocytes) were washed with PBS and incubated with fluorochrome-conjugated antibodies: Alexa Fluor® 488 Mouse Anti-Human CD14 and PE-CF594 Mouse Anti-Human CD16. The 3 subsets were separated based on their CD14 and CD16 expression levels (**Figure 1**).

After flow sorting, and within 6 hours of blood draw, the magnetic behavior of the monocytes and the metHb-RBCs was assessed in an instrument referred to as Cell Tracking Velocimetry (CTV) (Jin et al., 2008). CTV characterizes the magnetically induced velocity (u_m) and gravity induced settling velocity (u_s) in a region of interest, where a high, and well characterized magnetic gradient in the horizontal direction is created. Once the cells are injected, horizontal and vertical velocities are measured, which can be related to specific cellular and magnetic field properties. More specifically, the magnetically and gravitationally induced velocities, u_m and u_s , can be described as follows:

$$u_m = \frac{(\chi_{Cell} - \chi_{Fluid}) V_{Cell}}{3\pi D_{Cell} \eta} S_m$$

(1)

$$u_s = \frac{(\rho_{Cell} - \rho_{Fluid}) V_{Cell}}{3\pi D_{Cell} \eta} g$$

(2)

where subscripts cell and fluid refer to the cell and suspending fluid, χ is the magnetic susceptibility, ρ is the density, D and V are the diameter and volume of a cell (particle), η is the viscosity of the suspending fluid and g is the acceleration due to gravity (9.8 m/s^2). S_m , the magnetic energy gradient, is defined by:

$$S_m = \frac{|\nabla B^2|}{2\mu_0}$$

(3)

where μ_0 and B are the permeability of free space and the magnetic flux density at the source. When Equation (1) is divided by Equation (2), one obtains:

$$\frac{u_m}{u_s} = \frac{(\chi_{Cell} - \chi_{Fluid}) S_m}{(\rho_{Cell} - \rho_{Fluid}) g}$$

(4)

Note this ratio is no longer a function of the size (volume and diameter) of the cell nor the fluid viscosity (Park et al., 2019). Further rearranging leads to:

$$\chi_{Cell} = \chi_{Fluid} + \frac{u_m (\rho_{Cell} - \rho_{Fluid}) g}{u_s S_m} = \sum \phi_i \chi_i \quad (5)$$

As presented in Equation (5), the magnetic susceptibility of a cell is the sum of the magnetic susceptibilities of its constituents (χ_i) multiplied by the volume fraction of those constituents, ϕ_i . Whereas the cell is primarily composed of water and biomass, certain constituents, such as Fe^{2+} , Fe^{3+} , ferritin, etc., can increase the susceptibility of the cell such that the cell could experience positive magnetophoresis when suspended in PBS and in the presence of a magnetic field gradient.

Thus, in this work, after introducing the different monocyte subsets and metHb-RBCs into the CTV, images of the cells' movement were captured and processed using an in-house analysis program for calculating u_m and u_s . With these data, the cell magnetic susceptibility was also calculated.

To determine if any NK and B cells contaminated the non-classical subfraction, a sample was incubated with APC Mouse Anti-Human HLA-DR (see **Figure 2** to see the sorting procedure). Further, the purity of the sorted monocytes was also assessed on CTV for one sample by using dark field and fluorescence (with a 480 nm filter, to target the antibody conjugated to Alexa Fluor® 488) microscopy. More specifically, the current construction/operation of the CTV instrument requires that one chooses the filter set/optical setting for a given experiment. Consequently, two sets of experiments were conducted on one sample: a) the use of dark field optics, which allows all cells to be tracked, and b) a fluorescent filter set, compatible with the monocyte stain, CD14. Therefore, under the dark field mode all cells present in the channel were tracked, whereas under fluorescent mode only fluorescent cells, presumably monocytes bound with the anti-CD14 fluorochrome conjugate, were measured.

Statistical analysis of different subfraction of cells were evaluated using Mann-Whitney U tests and ANOVA on ranks tests (SigmaPlot, Systat Software, San Jose, CA). More specifically, differences in the magnetic velocity between several blood cells obtained from healthy donors were evaluated.

RESULTS

Figure 3 presents a dot plot for each of the three monocyte subtypes for the 5 donors, in terms of settling velocity versus magnetic velocity, and a secondary axis of magnetophoretic mobility. It should be first noted that magnetophoretic mobility is a method to “normalize” a specific experiment by dividing the measured magnetic velocity by the specific value of S_m (the driving force) used in the experiment. Above and on the right hand side of the dot plot, histograms of the data are presented. Also, an enlarged range is presented surrounding the highest number density of cells. Moreover, **Table 1** presents the comparisons between u_m and u_s of CD14⁺ cells from 10 donors (data modified from Kim et al. (2019)) and the five donors in this current study (Sample # 11-15). Inspection of the data for each donor indicates a significant variability in the mean magnetic velocity of the intermediate and non-classical monocytes; in contrast, the mean magnetic velocity of the classical monocytes is more consistent, and lower (presumably containing less iron) than the other two subtypes.

To provide a perspective on the value of these magnetic velocities/magnetophoretic mobilities to other cell types, **Figure 4** is presented. **Figure 4 a)** presents previously published values of the magnetophoretic mobility of peripheral blood lymphocytes, PBL, oxyHb-RBCs and methHb-RBCs (Chalmers et al., 2010; Kim et al., 2019). **Figure 4 b)** presents histograms of the three types of monocytes collected for this study, and **Figure 4 c)** presents the mobility of specimens of human glioblastoma (GBM) cells cultured in specific media (GBM no added Fe), and cultured with elevated iron concentrations (GBM added Fe) (Park et al., 2019). It can be observed that a significant fraction of the intermediate and non-classical monocytes have magnetophoretic mobilities equivalent to methHb-RBCs.

Moreover, the results obtained from our statistical analysis (**Tables S1 and S2**) suggest that all blood cell types obtained from healthy donors (RBCs, lymphocytes and monocytes, including monocyte subsets) are statistically different in terms of magnetic velocity ($p < 0.05$).

With respect to settling velocity (i.e. size), an unusual observation (both in this study, and in our previously published study (Kim et al., 2019)) was made (dot plot and histograms from **Figure 3**). We found that while the classical monocytes are the expected size, there are more than one size population of intermediate and non-classical monocytes. While at first thought a very low (and in some cases negative) settling velocity is hard to interpret (i.e. cells less dense than the suspending media), we have previously published that, for the operating conditions and equipment used in our current CTV (i.e. the magnetic energy gradient, the magnification, the pixel density of the CCD camera, and other operational settings), the standard error will increase significantly when the velocity value of a tracked cell/particle is in the range between 0.0005 mm/s and -0.0005 mm/s. To highlight this range in velocities, a cross hatched box was added to **Figure 3**. Nakamura et al. (2001) experimentally demonstrated that this degradation of accuracy of the CTV tracking algorithm occurs when the cell/particle movement approaches one pixel during the specific tracking interval. For the current experiments, this corresponds, approximately, to the area highlighted in the box.

While the actual size of entities within the box is indeterminate, similar small entities were found in our previous work, reported by Kim et al. (2019), after CD14 flow cytometry sorting, using a Coulter Counter size/concentration analyzer. Since many of these smaller entities still had significant magnetic velocity, Equation (5) was used to determine the magnetic susceptibility (volume susceptibility, which is dimensionless in SI units) of all of the cells and these small entities. It should be noted that the magnetic susceptibility is independent to the cell/entity size, and only a function of the concentration of the magnetic material within the cells/entity. **Figure 5** presents dot plots of the settling velocity as a function of the magnetic susceptibility of the cell/entity. It is quite clear that, for many, but not all, of the

intermediate and non-classical monocytes, as the cell gets smaller, the average magnetic susceptibility increases. As stated above, care needs to be taken in interpreting these results since the performance of CTV reporting settling velocity increases as the cell/particle travels more pixels in a given time. In fact, the lowest, non-zero velocity that CTV can detect is a velocity in which the center of the particle/cell moved 1 pixel over 5 sequential frames. To facilitate identifying this region of settling velocity, a shaded box is added to each of the panels reported in **Figure 5**. Nevertheless, a clear trend is apparent. **Table 2** presents the value obtained for the magnetic susceptibility of the three monocyte subsets (Samples 11-15).

Regarding the possible contamination of monocyte subsets with other cell types, such as lymphocytes, **Figure S1** presents a comparison between the reported velocities of sorted monocytes using CTV on dark field and fluorescence mode (with a 480 nm filter, to target the anti-CD14 antibody conjugated to Alexa Fluor® 488). It can be seen that CTV measured nearly identical u_m for cells under dark field and fluorescence imaging modes (5% discrepancy in the magnetic velocity). This result implies that the cells injected in the system were monocytes. Moreover, **Figure S2** presents an additional sample incubated with HLA-DR (to ensure that there was no contamination of non-classical cells with lymphocytes). This figure reveals the same results, that non-classical cells possess the highest magnetic velocity, followed by intermediate monocytes.

A comparison of the magnetic velocity between monocyte subtypes and the methHb-RBCs obtained from the same blood samples was additionally carried out. The results (**Figure 6**) suggest that the magnetic velocity of methHb-RBCs is similar for all samples, with an average velocity of 1 $\mu\text{m/s}$. Although for some samples (such as sample #15, see **Table 1**), non-classical monocytes reported a magnetic velocity as high as 2 $\mu\text{m/s}$, a high non-classical monocyte u_m is not correlated to a high methHb-RBCs velocity. Thus, there might not exist a relationship between the amount of iron in RBCs and the magnetic behavior of monocyte subsets. Based on these observations, and our recent publication on further characterization

of the mobility of RBCs (Kim et al., 2020), we suggest that these subsets have different magnetic and settling velocities due to their different physical properties; however, the RBC populations from the different donors report similar characteristics.

DISCUSSION

It is known that human monocytes are involved in iron recycling, but very little attention has been paid to their magnetic properties. In fact, monocytes have been considered “non-magnetic”, and different magnetic isolation techniques have been developed based on this assumption. In this study, we report the magnetic character of human monocytes by using CTV, which has the ability to track the movement of thousands of individual cells in response to an applied magnetic field. Our results confirm that the only monocyte subset that can be considered “non-magnetic” (i.e. its average magnetic susceptibility is not greater than that of water) is the classical subset, implying that non-classical and intermediate monocytes have higher iron storage capacities. This could, potentially, be attributed to at least two factors: i) the longer circulating half-lives of non-classical and intermediate monocytes, since they spend more time in circulation accumulating more iron from senescent RBCs (Kawamura & Ohteki, 2018), and/or ii) their inability to release iron for recycling. Regarding the second argument, a recent study has reported that classical monocytes expressed by far the highest levels of the surface protein ferroportin (the sole known mammalian iron export protein) among monocyte subpopulations (Haschka et al., 2019).

Our findings suggesting the paramagnetic behavior of monocytes in PBS have implications for the immunomagnetic separation industry. A fundamental criteria for any identification and/or separation technology is the ability to distinguish between the signal of the targeted entity and background noise. In the case of magnetic separation, especially when one is labeling the targeted cell with an antibody conjugated to a magnetic particle (i.e. MACS® MicroBead Technology from Miltenyi Biotec), one

assumes that the targeted, labeled cell has a higher magnetic mobility than the unlabeled cells. We have previously evaluated, and attempted to optimize, immunomagnetic labeling for both commercial magnetic cell separation systems (Miltenyi MACS system), as well as our own, flow-through separation systems (Comella et al., 2001; Melnik et al., 2001; Chosy et al., 2003; Lara et al., 2006; Zhang et al., 2006).

In the study by Melnik et al. (2001), which used fresh, human cord blood, and followed Miltenyi Biotec (Auburn, CA) protocols, it was recognized that the performance of the enrichment/recovery/purity of rare CD34⁺ cells from cord blood was inconsistent, and not optimal, when the results were evaluated using flow cytometry analysis of the feed and separated fractions. A number of reasons were suggested at the time for this suboptimum performance, including incomplete magnetic labeling of the targeted cells, and monocytes phagocytosing the magnetic particles (another study has reported significant magnetic mobilities of macrophages after phagocytizing magnetic particles (Pamme & Wilhelm, 2006)).

Figures 7 a) and **b)** present histograms of the magnetophoretic mobility of the unlabeled cord blood and the mobility of a positive fraction (twice separated in a MACS column) of the immunomagnetically labeled CD34 cells. It can be noticed, especially in the enlarged inset in **Figure 7 b)**, that an overlap in mobilities in the histograms of unlabeled and magnetically labeled cells exists. It is highly likely that magnetic monocytes were in the magnetically labeled fraction, which would then have stained negative for the CD34 flouoroprobe when evaluated with flow cytometry.

Another striking observation is the study by Comella et al. (2001). In this study, CD56⁺ cells were targeted in human peripheral blood lymphocytes, PBLs, using a two-step antibody labeling protocol; primary antibody: anti-CD56-PE conjugate, and a secondary anti-PE MACS bead conjugated (at the time Miltenyi Biotec did not make an anti-CD56 MACS bead conjugate). **Figure 7 c)** presents histograms of unlabeled PBLs, and various secondary antibody labeling amounts (per 10⁶ cells). **Figure 7 d)** presents the resultant magnetophoretic mobility as a function of the amount used of the secondary antibody.

One can clearly observe from **Figure 7 c)** that the peak of the immunomagnetically labeled cells moves to the right with increasing labeling amounts. In fact, the shift is so significant that a logarithmic scale on the x-axis is used. Several notable observations should be made. First, just as with the cord blood presented in **Figures 7 a)** and **b)**, the unlabeled cells have a small, but noticeable positive magnetic mobility populations, of similar mobility to the populations presented in this current study (**Figure 3**). Second, only when a high level of antibody-bead conjugate (much higher than is typically recommended) is used, is the overlap in mobilities removed.

We suggest that these results demonstrate that care should be taken when interpreting immunomagnetic separations. Obviously, immunomagnetic separations are widely popular, and in general very, effective. However, these results suggest that, depending on the type of separation conducted, “magnetic monocytes” could be present when one expects only magnetically labeled cells. Conversely, one might “lose” magnetic monocytes to the magnetic fraction, when expecting to recover all of the monocytes in the negative separation fraction (i.e. a depletion separation). The fact that these “magnetic” monocytes are only a fraction of all of the monocytes, and that monocytes are a relatively small fraction of all the nucleated cells in blood, indicates that this potential “magnetic monocyte” contamination is typically a small fraction of the targeted cell population. For example, Darabi & Guo (2006) reported a fraction of lost cells when trying to recover monocytes by using negative magnetic isolation techniques (they did not label the monocytes and assumed that they would be in the negative fraction), and this loss was more pronounced when the magnetic force was high (in comparison to the hydrodynamic drag force), which would be consistent with our current findings. While one might consider a Miltenyi MACS® column a low magnetic force separation, in fact, there is small zones within the column packing that have very high magnetic energy gradients, strong enough to be able to separate red blood cells without magnetic labeling, which would easily capture the magnetic monocytes that we have documented in this report. Moreover, Bhattacharjee et al. (2017) reported that monocytes isolated

with negative and positive magnetic sorting techniques showed different molecular characteristics and immunophenotypic behavior. They suggested that positive isolation affects functionality, but a comparison of CD14/CD16 levels in the recovered cells between the two methods was not carried out.

In contrast, a different study has suggested that the subset distribution does not significantly differ after monocytes are separated by negative depletion (Fendl et al., 2019). Since only a small percentage of monocytes are intermediate and non-classical, and a small fraction of these are slightly more magnetic than PBS, it is likely that the subset distribution does not vary much after negative depletion when employing low gradients and fields.

Another question to address is whether the magnetic properties of monocytes change for patients with blood diseases. The most important iron uptake mechanism of monocytes is phagocytosis of senescent RBCs (Kim et al., 2019). Thus, monocytes may contain higher iron concentration in patients suffering from RBC diseases, such as sickle cell anemia and β -thalassemia. Future studies will focus on addressing these questions and on the analysis of monocytes obtained from patients suffering from blood-related diseases.

ACKNOWLEDGMENTS

We wish to thank the National Heart, Lung, and Blood Institute (1R01HL131720-01A1) for financial assistance.

REFERENCES

Bhattacharjee, J., Das, B., Mishra, A., Sahay, P., & Upadhyay, P. (2017). Monocytes isolated by positive and negative magnetic sorting techniques show different molecular characteristics and immunophenotypic behavior. *F1000Research*, 6, Article 2045. doi: 10.12688/f1000research.12802.3

Chalmers, J. J., Xiong, Y., Jin, X., Shao, M., Tong, X., Farag, S., & Zborowski, M. (2010). Quantification of non-specific binding of magnetic micro- and nanoparticles using cell tracking velocimetry: Implication for magnetic cell separation and detection. *Biotechnology and Bioengineering*, 105, 1078–1093.

doi: 10.1002/bit.22635

Chosy, E. J., Nakamura, M., Melnik, K., Comella, K., Lasky, L. C., Zborowski, M., & Chalmers, J. J. (2003). Characterization of antibody binding to three cancer-related antigens using flow cytometry and cell tracking velocimetry. *Biotechnology and Bioengineering*, 82, 340–351. <https://doi.org/10.1002/bit.10581>

Comella, K., Nakamura, M., Melnik, K., Chosy, J., Zborowski, M., Cooper, M. A., Fehniger, T. A., Caligiuri, M. A., & Chalmers, J. J. (2001). Effects of antibody concentration on the separation of human natural killer cells in a commercial immunomagnetic separation system. *Cytometry*, 45, 285–293.

[https://doi.org/10.1002/1097-0320\(20011201\)45:4<285::AID-CYTO10018>3.0.CO;2-W](https://doi.org/10.1002/1097-0320(20011201)45:4<285::AID-CYTO10018>3.0.CO;2-W)

Darabi, J., & Guo, C. (2016). Continuous isolation of monocytes using a magnetophoretic-based microfluidic chip. *Biomedical Microdevices*, 18, Article 77. doi: 10.1007/s10544-016-0105-8

Fendl, B., Weiss, R., Eichhorn, T., Spittler, A., Fischer, M. B., & Weber, V. (2019). Storage of human whole blood, but not isolated monocytes, preserves the distribution of monocyte subsets. *Biochemical and Biophysical Research Communications*, 517, 709–714. <https://doi.org/10.1016/j.bbrc.2019.07.120>

Haschka, D., Petzer, V., Kocher, F., Tschurtschenthaler, C., Schaefer, B., Seifert, M., Sopper, S., Sonnweber, T., Feistritzer, C., Arvedson, T. L., Zoller, H., Stauder, R., Theurl, I., Weiss, G., & Tymoszyk, P. (2019). Classical and intermediate monocytes scavenge non-transferrin-bound iron and damaged erythrocytes. *JCI Insight*, 4, Article e98867. doi: 10.1172/jci.insight.98867

Jin, X., Zhao, Y., Richardson, A., Moore, L., Williams, P. S., Zborowski, M., & Chalmers, J. J. (2008). Differences in magnetically induced motion of diamagnetic, paramagnetic, and superparamagnetic microparticles detected by cell tracking velocimetry. *Analyst*, 133, 1767–1775. <https://doi.org/10.1039/B802113A>

- Kawamura, S., & Ohteki, T. (2018). Monopoiesis in humans and mice. *International Immunology*, 30, 503–509. <https://doi.org/10.1093/intimm/dxy063>
- Kim, J., Gómez-Pastora, J., Weigand, M., Potgieter, M., Walters, N. A., Reátegui, E., Palmer, A. F., Yazer, M., Zborowski, M., & Chalmers, J. J. (2019). A subpopulation of monocytes in normal human blood has significant magnetic susceptibility: Quantification and potential implications. *Cytometry Part A*, 95, 478–487. <https://doi.org/10.1002/cyto.a.23755>
- Kim, J., Gómez-Pastora, J., Gilbert, C. J., Weigand, M., Walters, N. A., Reátegui, E., Palmer, A. F., Yazer, M., Zborowski, M., & Chalmers, J. J. (2020). Quantification of the mean and distribution of hemoglobin content in normal human blood using cell tracking velocimetry. *Analytical Chemistry*, 92, 1956–1962. <https://doi.org/10.1021/acs.analchem.9b04302>
- Kratofil, R. M., Kubes, P., & Deniset, J. F. (2017). Monocyte conversion during inflammation and injury. *Arteriosclerosis, Thrombosis, and Vascular Biology*, 37, 35–42. <https://doi.org/10.1161/ATVBAHA.116.308198>
- Lara, O., Tong, X., Zborowski, M., Farag, S. S., & Chalmers, J. J. (2006). Comparison of two immunomagnetic separation technologies to deplete T cells from human blood samples. *Biotechnology and Bioengineering*, 94, 66–80. DOI: 10.1002/bit.20807
- Marimuthu, R., Francis, H., Dervish, S., Li, S. C. H., Medbury, H., & Williams, H. (2018). Characterization of human monocyte subsets by whole blood flow cytometry analysis. *Journal of Visualized Experiments*, 140, Article e57941. doi: 10.3791/57941
- Melnik, K., Nakamura, M., Comella, K., Lasky, L. C., Zborowski, M., & Chalmers, J. J. (2001). Evaluation of eluents from separations of CD34⁺ cells from human cord blood using a commercial, immunomagnetic cell separation system. *Biotechnology Progress*, 17(5), 907–916. <https://doi.org/10.1021/bp010079r>

Nakamura, M., Zborowski, M., Lasky, L. C., Margel, S., & Chalmers, J. J. (2001). Theoretical and experimental analysis of the accuracy and reproducibility of cell tracking velocimetry. *Experiments in Fluids*, 30, 371–380. <https://doi.org/10.1007/s003480000211>

Pamme, N., & Wilhelm, C. (2006). Continuous sorting of magnetic cells via on-chip free-flow magnetophoresis. *Lab on a Chip*, 6, 974–980. DOI: 10.1039/b604542a

Park, K. J. J., Kim, J., Testoff, T., Adams, J., Poklar, M., Zborowski, M., Venere, M., & Chalmers, J. J. (2019). Quantitative characterization of the regulation of iron metabolism in glioblastoma stem-like cells using magnetophoresis. *Biotechnology and Bioengineering*, 116, 1644–1655. doi: 10.1002/bit.26973

Sprangers, S., de Vries, T. J., & Everts, V. (2016). Monocyte heterogeneity: Consequences for monocyte-derived immune cells. *Journal of Immunology Research*, 2016, Article 1475435.
doi: 10.1155/2016/1475435

Weiss, G. (2009). Iron metabolism in the anemia of chronic disease. *Biochimica et Biophysica Acta*, 1790, 682–693. doi: 10.1016/j.bbagen.2008.08.006

Zhang, H., Williams, P. S, Zborowski, M., & Chalmers, J. J. (2006). Binding affinities/avidities of antibody-antigen interactions: Quantification and scale-up implications. *Biotechnology and Bioengineering*, 95, 812–829. DOI: 10.1002/bit.21024

TABLES

Table 1. Magnetic (u_m) and gravitational settling (u_s) velocities of human CD14⁺ monocytes (Sample # 1-10; data modified from Kim et al. (2019)) and human monocyte subsets, classical, intermediate and non-classical (Sample # 11-15).

Sample #	Analyzed CD14 ⁺ cells	$u_m \pm \text{SD}$ ($\mu\text{m/s}$)	$u_s \pm \text{SD}$ ($\mu\text{m/s}$)	% of cells with $u_m < 0$	% of cells with $u_m > 0$
1	161	2.21 ± 5.14	1.24 ± 0.70	23	77
2	191	6.67 ± 6.29	0.86 ± 1.10	1	99
3	337	5.16 ± 8.42	1.25 ± 1.58	24	76
4	1159	1.01 ± 3.58	1.22 ± 0.62	57	43
5	109	4.88 ± 6.81	0.70 ± 1.90	2	98
6	118	0.51 ± 1.31	-0.13 ± 0.60	26	74
7	165	0.89 ± 2.94	0.83 ± 2.32	41	59
8	195	2.10 ± 3.10	-0.05 ± 0.97	21	79
9	126	0.38 ± 2.05	0.90 ± 1.33	60	40
10	310	0.06 ± 1.45	1.23 ± 0.97	75	25

Average 1-10	2871 [†]		2.00 ± 5.00	1.00 ± 1.20	43	57
Sample #	Classical (3385 cells)		Intermediate (1461 cells)		Non-classical (847 cells)	
	$u_m \pm SD$ ($\mu\text{m/s}$)	$u_s \pm SD$ ($\mu\text{m/s}$)	$u_m \pm SD$ ($\mu\text{m/s}$)	$u_s \pm SD$ ($\mu\text{m/s}$)	$u_m \pm SD$ ($\mu\text{m/s}$)	$u_s \pm SD$ ($\mu\text{m/s}$)
11	-0.24 ± 0.58	1.5 ± 0.63	0.19 ± 1.13	1.02 ± 0.77	-0.13 ± 0.58	1.14 ± 0.89
12	-0.17 ± 1.49	1.53 ± 0.51	0.35 ± 1.59	0.58 ± 0.79	0.63 ± 1.58	0.34 ± 0.57
13	-0.7 ± 0.98	1.36 ± 0.51	0.23 ± 1.47	1.21 ± 0.83	0.66 ± 3.79	0.97 ± 0.80
14	-0.37 ± 0.61	1.22 ± 0.50	0.49 ± 1.16	0.52 ± 0.76	0.38 ± 1.04	0.54 ± 0.86
15	-0.16 ± 0.41	1.38 ± 0.53	1.19 ± 3.47	0.77 ± 1.41	2.16 ± 7.69	-0.07 ± 1.05
Average 11-15	-0.30 ± 0.76	1.39 ± 0.56	0.39 ± 1.75	0.89 ± 0.92	0.47 ± 2.59	0.68 ± 0.88

[†] Total number of CD14⁺ cells analyzed

Table 2. Magnetic susceptibility of human monocyte subsets, classical, intermediate and non-classical (Sample # 11-15). Whereas all the cell types report negative magnetic susceptibilities, the difference in the susceptibility between the cell and the fluid (PBS) is positive for some of the intermediate and non-classical subsets. This implies that these cells will experience positive magnetophoresis when suspended in PBS and in the presence of a magnetic field gradient.

Sample #	Classical		Intermediate		Non-classical	
	$\chi_{\text{cell}} \times 10^6$	$\chi_{\text{cell}} - \chi_{\text{fluid}} \times 10^6$	$\chi_{\text{cell}} \times 10^6$	$\chi_{\text{cell}} - \chi_{\text{fluid}} \times 10^6$	$\chi_{\text{cell}} \times 10^6$	$\chi_{\text{cell}} - \chi_{\text{fluid}} \times 10^6$
11	-9.63	-0.58	-10.64	-1.59	-12.86	-3.81
12	-10.59	-1.54	13.20	22.25	-45.28	-36.23
13	-11.29	-2.24	-8.53	0.52	-5.81	3.24
14	-10.37	-1.32	-4.86	4.19	-0.97	8.08
15	-9.83	-0.78	-12.29	-3.24	-11.10	-2.05
Average	-10.17	-1.12	-7.79	1.26	-12.52	-3.47

FIGURE LEGENDS

Figure 1. Sample preparation procedure. First, human fresh whole blood was separated into three fractions by density gradient centrifugation: i) plasma, ii) RBCs (oxyhemoglobin RBCs), and iii) PBMCs. The PBMCs were further processed by FACS targeting for monocyte subsets based on their different CD14 and CD16 expression levels. MetHb-RBCs were obtained by treating the oxyHb-RBCs with NaNO_2 . Afterward, the different populations were magnetically characterized on CTV. The samples were processed within 6 h of blood draw.

Figure 2. Flow sorting results for monocyte isolation from one sample. a) FSC(A) vs. FSC(H) plot: Removal of doublets, clumps and debris by gating the cells that have an equal area and height; b) FSC(A) vs. SSC(A) plot: Selection of monocytes based on their SSC/FSC properties; c) CD16 vs. CD14 plot: Gating to

select monocytes; d) CD16 vs. HLA-DR plot: Gating to select HLA-DR positive cells and remove NK cells; e) CD14 vs. HLA-DR: Gating to exclude the B cells (HLA-DR high/CD14 low) from the monocytes; f) Gating monocyte fractions based on CD14 and CD16 expression levels (P7 are classical, P8 are non-classical and P9 are intermediate). HLA-DR (steps d) and e)) was only included in one sample to evaluate the possible contamination of non-classical monocytes, but the other steps were performed for all the samples.

Figure 3. CTV analysis of the monocyte subtypes. Dot plot showing the magnetic and settling velocities of individual cells, as well as the magnetophoretic mobility. Histograms are presented above and on the right of the dot plot. On the right top of the figure, an enlarged range is presented surrounding the highest number density of cells (the cross hatched box indicates the range of velocities where the standard error is the highest).

Figure 4. Magnetophoretic mobilities of blood cells obtained from healthy donors and cancer cells cultured in different media. a) Lymphocytes (PBL) and oxyHb-RBCs and methHb-RBCs; b) Subsets of monocytes collected for this study; c) Glioblastoma (GBM) cells cultured in a media containing and not containing iron.

Figure 5. Settling velocity (proportional to the size of the cells) as a function of the volumetric magnetic susceptibility. a) Classical monocytes; b) Intermediate monocytes; c) Non-classical monocytes. The cross hatched boxes indicate the range of velocities where the standard error is the highest.

Figure 6. Magnetic velocity of the methHb-RBCs from sample # 11-15. The numbers inside the graphs show the average magnetic velocity \pm a 95% confidence interval.

Figure 7. Implication of the presence of magnetic monocytes in the immunomagnetic separation of other cells. a) and b) Immunomagnetic separation of CD34 positive cells, adapted from Melnki et al. (2001): Histograms of the magnetophoretic mobility of unlabeled (gray) and immunomagnetic labeled cells after separation (note the overlap in mobilities); c) and d) CD56 separation from PBLs (Comella et al., 2001): the amount of the secondary label (anti-PE MACS bead conjugate), in $\mu\text{L}/10^6$ cells is presented. Since the magnetophoretic mobility is greatly increased as the amount of label is increased, the x-axis in Figure 7 c) and y-axis in Figure 7 d) are presented in log scale.